



Research Article

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## Magnetic and corrosion properties of 316L and 316LVM after high temperature gas nitriding

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### ABSTRACT

Recently, biocompatibility is not only concern to the metallic biomaterial, but also MRI safety and compatible, should be considered. If the corrosion resistance may be used as the biocompatibility requirements, MRI safety and compatibility need a stable non-magnetic metallic biomaterial. The improvements of austenitic stainless steel 316L and 316LVM by low temperature nitriding results weakly magnetic properties which lead to MRI unsafe and incompatible due to the formation of M-nitride. High temperature gas nitriding promises for enhancing corrosion resistance without generate M-nitride. HTGN treatments for 316L and 316LVM are successfully done at temperature 1050 °C and 15 minutes holding time. Polarization test by vibrating sample magnetometer (VSM) and XR diffraction confirm that the HTGN treatments able to improve corrosion resistance and enhance the non-magnetic properties of both 316L and 316LVM.

**Keywords:** MRI safety and compatible, HTGN, 316L and 316LVM

### INTRODUCTION

Austenitic stainless steel 316L and 316LVM are ones of metallic biomaterial that widely used as implants and medical devices. They have high corrosion resistance and good mechanical properties. Corrosion resistance of metallic biomaterials can be used as the parameter of their biocompatibility. High corrosion resistance is more biocompatible. However, in the corrosive body fluid mediums, lack of oxygen and high load such as bone fixation the corrosion resistance of 316L and 316LVM decrease. Corrosion products cause any adverse effects to the body [1].

Various surface treatments such as gas nitriding, ion implantation, and plasma nitriding have been successfully applied to enhance their corrosion resistance. These treatments usually have been conducted at low temperature or below the austenite temperature. Low temperature nitriding produces thin layer of expanded austenite phase which improve their hardness and corrosion resistant. This expanded austenite phase is ferromagnetic [2, 3]. Furthermore this phase cause weakly ferromagnetic properties of nitride austenitic stainless steel.

Recently, increasing of corrosion resistance is not only concern for improvement of metallic biomaterial but also stable non-magnetic properties. The development magnetic resonance imaging (MRI) as clinical imaging tools needs metallic biomaterial that has stable non-magnetic properties. The principal issues for MR safety and compatibility are magnetically induced displacements and torque, radio frequency (RF) heating and image artifact [4]. Implanted and medical devices from austenitic stainless steel meet the MRI safety and compatibility in the up to 1.5T systems. However the developments of new 3.0T MR system cause their MR compatibility being decrease [5, 6].

The improvement of corrosion resistance of austenitic stainless steel by low temperature nitriding which produce expanded austenite phase should be avoided due to the MR safety and compatibility issues. Another method which

promises the improvement of corrosion resistance of austenitic stainless steel without produce expanded austenite phase or another ferromagnetic phase such as (Fe, Cr, Mo)N is high temperature gas nitriding (HTGN) [7]. HTGN treatment is thermo chemical process which able to diffuse the nitrogen atom into stainless steel. Hardness and corrosion resistance significantly improve by this treatment.

The early work for elimination the magnetic properties using HTGN treatment has developed. Weakly magnetic properties of free nickel high nitrogen austenitic stainless steel due the present of delta ferrite can be eliminated by HTGN treatments [8]. Although HTGN treatment for stainless steel has been investigate by many researchers [7, 9, 10] but the effect of HTGN treatments on the magnetic behavior of 316L and 316LVM not yet investigation. This papers deal with the effect of HTGN treatment on the corrosion and magnetic properties of 316L and 316LVM.

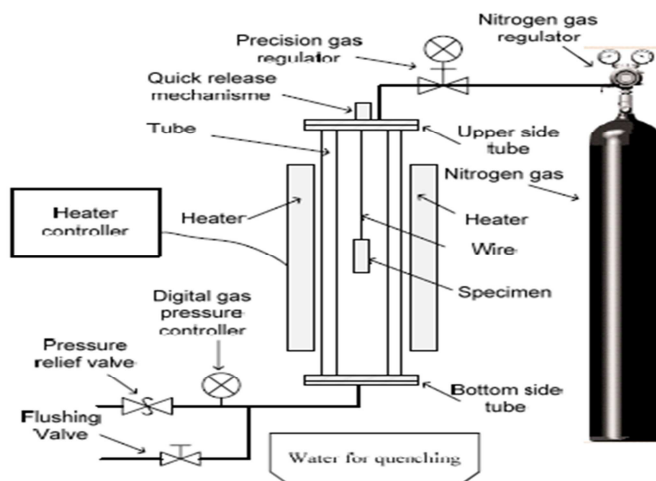
## EXPERIMENTAL SECTION

Specimens were prepared from 316L and 316LVM plate. The chemical compositions of the specimens are shown in table 1. Specimens were rinsed using ultrasonic cleaner in acetone as soaking medium prior HTGN treatments in order to remove oil and debris. HTGN treatments were carried out at modified three zone heating chamber of vertical furnace (Carbolite® type TZF 15/50/610). The furnace equipped with a precision digital pressure controller in order to maintain the pressure in the tube during treatments. Fig. 1 shows the HTGN furnace that used during treatments.

**Table 1. Chemical composition of specimens (%wt)**

	C	Cr	Ni	Mo	Mn	Si	Fe
316L	0.01	15.5	11.8	1.24	1.23	0.47	balance
316LVM	0.01	17.3	15.5	1.73	1.67	0.42	balance

Specimens were inserted to the furnace tube, vacuumed to 10 Pa for 15 minute then flushed using nitrogen gas at 1000 ml/min for 15 minute prior heated. Nitrogen gas flowed continuously at 100 ml/min until treatment temperatures achieved. During process, the pressure inside the furnace tube maintained at 0,3atm. The temperature treatment was chosen at 1050 °C and holding time for 15 minutes. This temperature and holding time were selected as optimum process variables resulted from previous experiments [11]. After heating process, specimen was quenched in the water.



**Fig. 1. Modified three zone Carbolite® furnace for HTGN treatments**

As received and treated specimens were cut and machined to produce 1.4 mm disc. The discs were gently polished in order to remove the scale using metal polish. These discs produced 1 cm<sup>2</sup> area in the corrosion test. The discs were rinsed by acetone prior corrosion test. The corrosion test was carried out at the surface of disc using polarizations resistance corrosion techniques in ringer solution as corrosion medium at temperature 37°C. For the first running test, the initial potential test and final was selected -20mV vs E<sub>corr</sub> and +20mV vs SCE respectively and the potential scan rate was 0.1mV. Each specimen tested for three times to determined I<sub>corr</sub>.

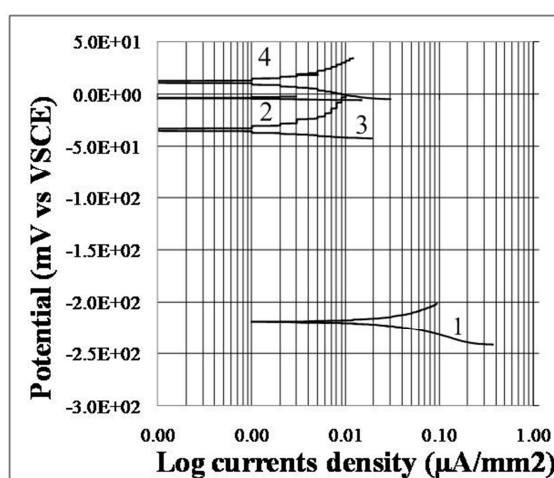
Magnetic properties were evaluated using vibrating sample magnetometer (VSM). As received and treated specimens processed in to powder using low speed saw before test. VSM test conducted by means exposure the powder in the magnetic field from -1 to 1 T. Magnetic moment (emu) recorded during VSM test.

After HTGN treatments, treated specimens 316L and 316LVM were evaluated by XRD. The XRD test conducted at Shimadzu type 7000s. Scan range was chosen at  $10 - 90^\circ$  and scan speed 2degree/min. XRD spectrum compared with crystallography open database (COD).

## RESULTS AND DISCUSSION

Fig. 2 shows the polarization curve obtained from corrosion test. Polarization curve for treated specimen both 316L and 316LVM are shift to up and left. It indicates that treated specimen has more corrosion resistance than as-received ones. Corrosion resistance of as received 316LVM is higher than as-received 316L. However, the corrosion resistance for treated specimen of 316L is close to the as received 316LVM. It indicates that HTGN treatment is able to enhance the corrosion resistance of 316L.

Table 2 show the  $E_{\text{corr}}$  and  $i_{\text{corr}}$  for as-received and treated specimens. Corrosion resistance of as received 316L increases from 0.0228mpy up to 0.0011mpy after HTGN treatment. Corrosion resistance of as received 316LVM increases from 0.0013 up to 0.0002mpy after treatments. The increasing of corrosion resistance produced by HTGN treatments of 316L is higher than for 316LVM. HTGN treatment for 316L is more effective to increasing the corrosion resistance than 316LVM.

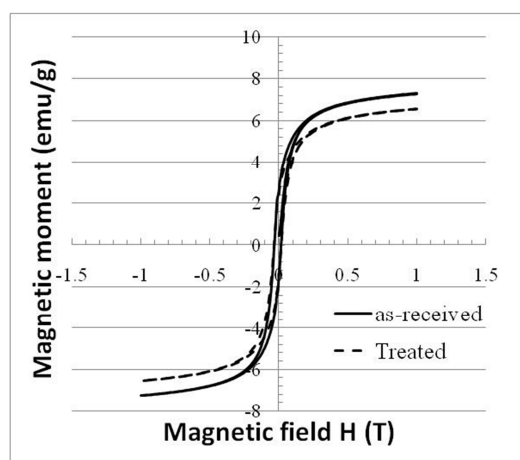


**Fig. 2. Polarization curve of as-received and treated specimens**

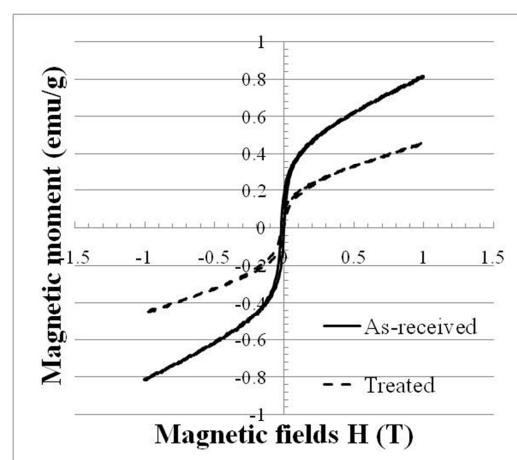
1: as-received 316L, 2: treated 316L, 3: as-received 316LVM & 4: treated 316LVM

**Table 2. Potential corrosion and  $i_{\text{corr}}$  of 316L and 316LVM**

Specimens	$E_{\text{corr}}$ (mV)	$i_{\text{corr}}$ ( $\mu\text{A}/\text{cm}^2$ )	Corrosion rate (mpy)
316L	As-received	-218.46	0.06
	Treated	-119.48	0.00040
316LVM	As-received	-33.43	0.00041
	Treated	-39.11	0.00006



a. 316L



b. 316LVM

**Fig. 3. Magnetization curve of specimens**

Fig. 3 shows the magnetization curve from VSM test. As received 316LVM has magnetization curve is lower one-per-tenth compared to the as-received 316L. It indicates that vacuums melting not only enhance the corrosion resistance but also improve the non-magnetic properties of 316LVM. Fig. 3 shows that after HTGN treatments, the magnetization curve both 316L and 316LVM is lower than as-received specimens. It indicates that HTGN not only increase the corrosion resistance but also improve the stable non-magnetic phase.

Fig. 4 shows the XRD spectrum of the specimens at the surface after HTGN treatments. The strongest peak obtained at  $43.6^\circ$ ,  $50.7^\circ$  and  $74.6^\circ$  which indicate the austenite phase. HTGN treatments for 316L and 316LVM do not change the initial phase of that steel. The only phase which present at micro structure is austenite.

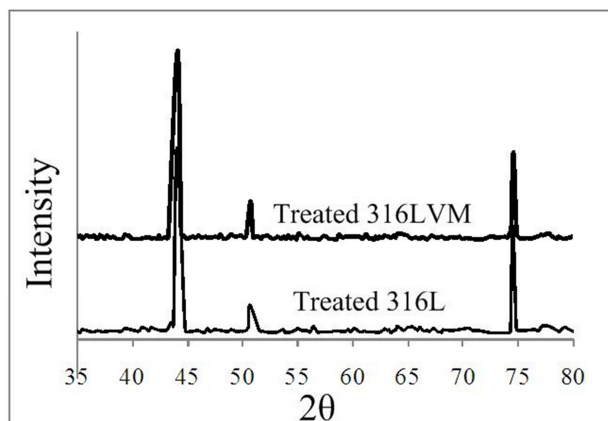


Fig. 4. XRD spectrum of treated specimens

The corrosion resistance of stainless steels may predicted by pitting resistance equivalent number (PREN). The magnitude of PREN only depends on the chemical composition of stainless steel mainly for Cr, Mo and N. The corrosion resistance increase with PREN. The formulae of PREN is  $\%Cr + 3.3\%Mo + (20 - 30)\%N$ . The chemical composition of 316L and 316LVM is not significantly different. There for the magnitude of PREN is also identically. However, the corrosion resistance of stainless steel actually not only depends on the chemical composition but also the cleanliness and homogeneity of their micro structure. Corrosion resistance increases with cleanliness and homogeneity.

Although the magnitude of PREN for 316L and 316LVM is not significantly different, the corrosion resistance of as received 316LVM is higher than as received 316L. Type 316LVM is produced by remelting 316L in the vacuum environment. The vacuum casting process produces micro structures which increase cleanliness and homogeneity [12, 13]. Segregation and impurity are significantly reduced and lead to higher corrosion resistance.

Treated 316LVM has corrosion resistance close to the as-received 316LVM as indicate that polarization curve is close each other. Corrosion process do at the surface, there for the increasing corrosion resistance depends on the chemical composition and the micro structure at the surface. HTGN treatments increase the nitrogen contents. The diffusion process starts at the surface. The nitrogen contents immediately increase at the surface. The increasing nitrogen contents at the surface cause the increasing of PREN and increasing the corrosion resistance of the specimens.

Fig 4 shows that the austenite is only phase on micro structure at the surface. It indicates that nitrogen atoms are interstitially solid solution in the austenite phase. Increasing corrosion resistance of treated specimens depends solely on the increasing of nitrogen contents. However, the corrosion resistance of treated 316L is close to the as-received and treated 316LVM. This phenomenon may results from improvement of cleanliness and homogeneity of treated 316L specimens. The early work to elimination of weakly magnetic properties shows that the HTGN treatment is able to dissolve the other phase into austenite phase [8].

Non magnetic properties of 316L and 316LVM are resulted from austenite phase. In the Fe-C alloys, austenite phase is only present at high temperature. The addition of austenite stabilizer elements such as Ni, Mn and N cause the austenite phase stable until room temperature. However, this phase may transform into martensite phase if excessive cold working being applied. Martensite phase has strong ferromagnetic properties. The present of martensite phase at the austenitic stainless steel change the non-magnetic into weakly magnetic properties. The present of the other phase in austenitic stainless steel such as M-nitride such as (Fe, Cr, Mo)N also have the same effect with martensite phase.

As shown at fig. 3, the magnetization curve both treated specimens for 316L and 316LVM shows reduced the magnetic moments. It indicate that HTGN treatment not only increase the corrosion resistance but also improve the non-magnetic properties. Although the initial phase of both as-received 316L and 316LVM is austenite, the magnetic moment for as received 316LVM has the order one per tenth than 316L. It indicates that the 316LVM has more stable austenite phase than 316L due to the higher nickel contents as shown at table 2.

The magnetization curve of 316L and 316LVM reduce after HTGN treatments. As the austenite phase is the only phase at the specimens as shown in fig. 4, the reduced of magnetization curve is caused by the increasing nitrogen contents at the specimens. Nitrogen is austenite stabilizer elements, increasing the nitrogen contents lead in to austenite more stable.

The reduced magnetic moments is also indicates that the HTGN treatments does not produce the formation of (Fe, Cr, Mo)N which may presents due to the increasing the nitrogen contents. The increasing nitrogen content is limited to the solubility of austenite phase. After solubility limit is achieved, nitrogen atom's can not continue to diffuse to the stainless steel. The solubility limit of nitrogen cause the formation of M-nitride can not be obtained by HTGN treatments for austenitic stainless steel. The results of XRD test confirm that after HTGN treatments, austenite is the only phase which present at the specimens.

### CONCLUSION

HTGN treatments for austenitic stainless steel 316L and 316LVM at treatments temperature 1050 °C for 15 minutes enhanced both corrosion resistance and non-magnetic properties. The improving non-magnetic properties after treatments because HTGN can dissolve the magnetic phase, does not produces (Fe, Cr, Mo)N compounds and increasing the nitrogen contents as austenite stabilizer elements. The enhancing of corrosion resistance and non magnetic properties indicates that treated specimens are more biocompatible and more MR safe and compatible than as-received samples.

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