



Research Article

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Landweber iteration algorithm based on sensitivity updating strategy for electrical capacitance tomography

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ABSTRACT

Electrical capacitance tomography (ECT) is a technique developed in recent years, which aims to measure multi-phase flow. The quality of reconstructed images is the bottleneck for its successful applications. Sensitivity matrix is calculated based on the known permittivity distributions, which is necessary in the most common used sensitivity-based image reconstruction algorithms of ECT. It is assumed that sensitivity matrix will hardly be affected by flow regimes. As a result, the fixed sensitivity matrix was used during the image reconstruction. However, there exists 'soft-field' effect and the sensitivity matrixes are changeable corresponding to different flow regimes, which results the decrease of reconstructed image quality. Therefore, Landweber iterative algorithm with updated sensitivity matrix was studied in this paper to improve the quality of reconstructed images. The initial image for sensitivity matrix update was obtained by Landweber iterative algorithm, and the results of different sensitivity matrix update intervals were compared. The times of sensitivity matrix updating were also analyzed. Experimental and simulation results showed that reconstructed images with higher accuracy can be obtained.

Key words: Electrical capacitance tomography; Image reconstruction; Landweber iteration; Sensitivity matrix update

INTRODUCTION

Electrical capacitance tomography (ECT) is one kind of process tomography techniques which was developed during the late 1980s [1, 2]. ECT technique has been investigated extensively during the past decades as a visualization technique for measurement and imaging of two-phase flows in real time in industrial process monitoring [3-5]. The task of image reconstruction for ECT is to determine the permittivity distribution and hence material distribution over the cross-section using the capacitance measurements.

However, there are three difficult problems in image reconstruction, termed as 'soft-field' effect, underdetermined problem and ill-posed inverse problem [6]. In general, image reconstruction algorithms can be divided into two classes [7]. One is non-iterative algorithm such as linear back projection (LBP) algorithm, which is fast in speed and suitable for online imaging, but, the quality of the reconstructed images is low. The other is iterative algorithm such as Landweber iterative algorithm which can provide quantitative images. The sensitivity matrix is generally needed for all the algorithms of both classes [8-10].

Usually, the sensitivity matrix is calculated with a selected reference permittivity distribution, assuming that the media distribution doesn't affect the electrical potential distributions. There exists 'soft-field' effect and the media distribution will greatly affect the electrical potential distributions. For different electrodes and locations, this affection is different. As a result, the sensitivity matrix will change with the media distribution and needs to be updated. To enhance the quality of the reconstructed images, sensitivity matrix updating strategy is considered in this paper.

In principle, sensitivity matrix should be updated according to the true media distribution, which is unknown. Therefore, sensitivity matrix can only be updated according to the reconstructed image by some reconstruction algorithms, say, Landweber iterative algorithm. A modified Landweber iterative algorithm based on updated sensitivity matrix was presented in this paper. The reconstructed image based on conventional Landweber iteration was selected as the initial image for sensitivity matrix update, and the reconstructed images after sensitivity matrix update using different initial images were compared. The effect on the quality of reconstructed images for different times of sensitivity matrix update was also analyzed. Simulation and static test results showed that reconstructed images with higher accuracy can be obtained.

PRINCIPLE OF ECT

ECT technique involves a number of capacitive electrodes mounted circumferentially around a flow pipe, and relies on changes in capacitance values between electrodes owing to the change in permittivity of flow components, as is shown in figure 1.

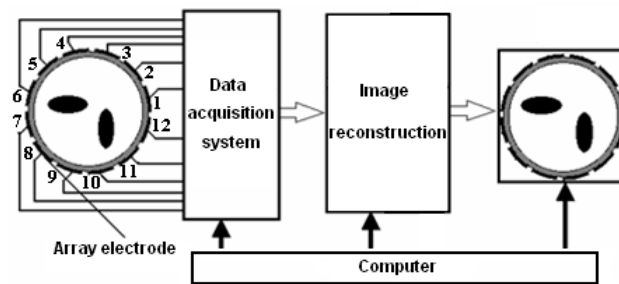


Fig. 1: Principle diagram of ECT system

The electrical field inside an ECT sensor can be calculated using the Laplace equation which is given by

$$\nabla \cdot [\varepsilon(x, y) \nabla u(x, y)] = 0 \quad (1)$$

where $\varepsilon(x, y)$ is the permittivity distribution in the sensing field, $u(x, y)$ is the potential distribution. The relationship between capacitance C and $\varepsilon(x, y)$ is governed by the following equation

$$C = \frac{Q}{V} = -\frac{1}{V} \oint_{\Gamma} \varepsilon(x, y) \nabla u(x, y) d\Gamma \quad (2)$$

where Q is the charge of an electrode, V is the potential difference between an electrode pair and Γ is the electrode surface.

Capacitances are measured between different electrode pairs and the measurements obtained are used to reconstruct a cross sectional distribution of flow components. For a 12-electrode system, the number of independent capacitance measurements is 66.

Landweber iterative algorithm is one of the widely used iterative algorithms for ECT. Landweber iterative algorithm is defined as [11, 12]

$$\begin{cases} G_{k+1} = G_k + \eta S^T (\lambda - S G_k) \\ G_0 = S^T \lambda \end{cases} \quad (3)$$

where G_k is the normalized image grey in the k th iteration. λ is the normalized capacitance vector, S is the sensitivity matrix which is defined as

$$S_{ij}(k) = \mu(k) \cdot \frac{C_{ij}^m(k) - C_{ij}^l}{C_{ij}^h - C_{ij}^l} \cdot \frac{1}{\varepsilon_h - \varepsilon_l} \quad (4)$$

where ε_h and ε_l are high and low permittivity values, C_{ij}^h and C_{ij}^l represent capacitance of electrode pair

$i-j$ when the pipe is full of high and low permittivity material, respectively. C_{ij}^m is the measurement capacitance of electrode pair $i-j$ when the k th element has high permittivity and the other elements have low permittivity. $\mu(k)$ is a correction factor related to the area of the k th in-pipe element.

LANDWEBER ITERATIVE ALGORITHM WITH UPDATED SENSITIVITY MATRIX

The Landweber iterative algorithm with updated sensitivity matrix can be expressed as figure 2. The block in dash line is conventional Landweber iterative algorithm. While for the modified Landweber iterative algorithm with updated sensitivity matrix, the initial image is obtained by the conventional Landweber iterative algorithm [13].

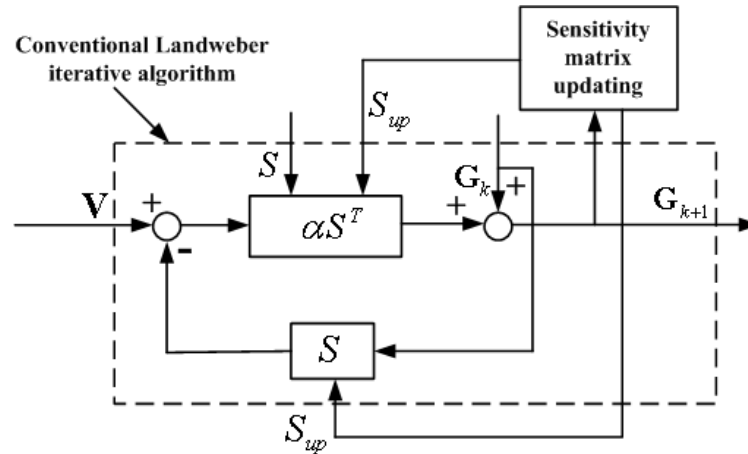


Fig. 2: Landweber iterative algorithm with updated sensitivity matrix

The Landweber iteration algorithm with updated sensitivity matrix can be expressed as

$$\begin{cases} G_{k+1} = G_k + \eta S_{up}^T (\lambda - S_{up} G_k) \\ G_0 = G_m \text{ (Conventional Landweber)} \end{cases} \quad (5)$$

Where G_0 is the reconstructed image after m times iterations of conventional Landweber iterative algorithm, which is used as the initial image for sensitivity matrix update. S_{up} is the updated sensitivity matrix.

EXPERIMENTS AND RESULTS

SIMULATIONS

Simulation experiment was carried out on a PC with Pentium™ 2.9 GHz and 512 M memory using the software developed by Tianjin University with MATLAB 2007. A 16-electrode ECT sensor was adopted and the mesh grid was shown in figure 3. The parameters of ECT sensor and mesh were listed in Table 1.

Table 1. Parameters of sensor and mesh

Parameters	Values
Inner diameter of sensor	160 mm
Number of electrodes	16
Reference relative permittivity	1
Number of elements	1920
Number of nodes	1057

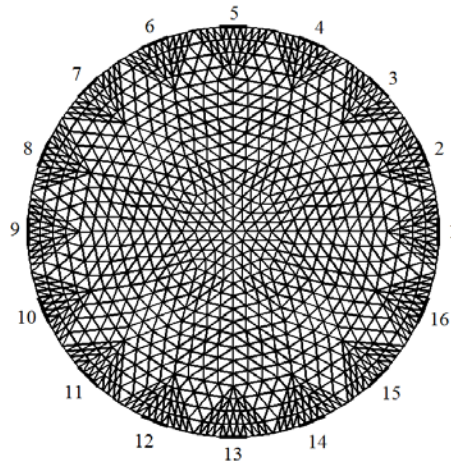


Fig. 3: Mesh grid

To compare the reconstructed images quantitatively, the relative image error (RE) was used.

$$RE = \frac{\|\sigma^* - \sigma\|_2}{\|\sigma\|_2} \quad (6)$$

Where σ and σ^* are the real and reconstructed permittivity distributions, respectively.

COMPARISON OF DIFFERENT INITIAL IMAGE FOR SENSITIVITY MATRIX UPDATE

The initial image for sensitivity matrix update is important, which is selected by experience. In this paper, reconstructed images of 10th, 50th and 100th iteration of conventional Landweber iterative algorithm were selected as the initial images for the sensitivity matrix update, and the reconstructed images until 200th iterations after 1st sensitivity matrix update were compared. Simulation results were shown in figure 4.

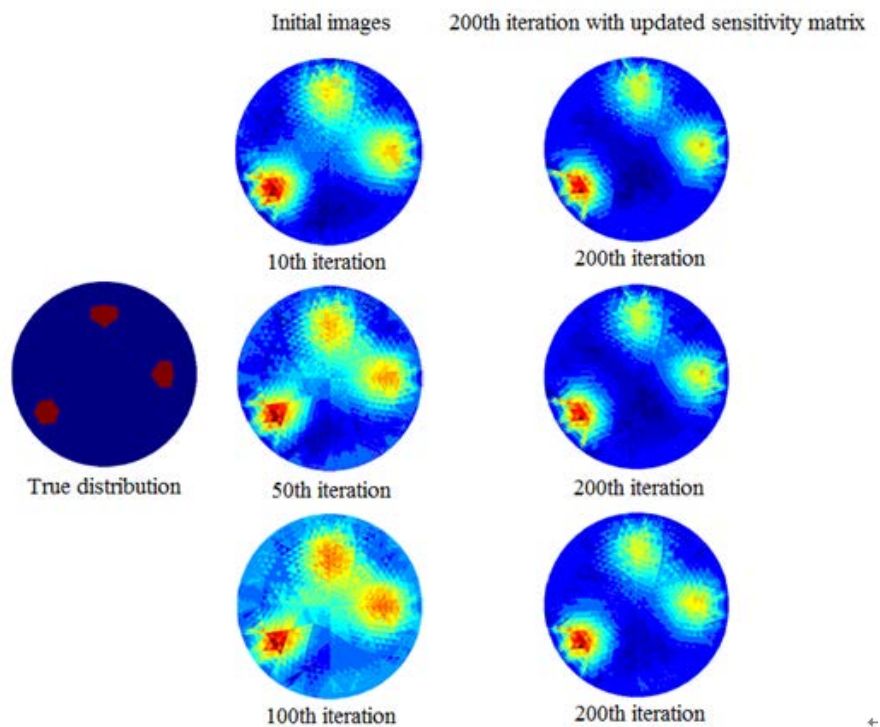


Fig. 4: Different initial images for sensitivity matrix update

Figure 5 shows the behavior of RE, which consists of both initial iteration (conventional Landweber iterative algorithm) and 200 iterations using updated sensitivity matrix for the considered phantoms. It can be seen from

figure 5 that the RE of the initial image at 50th iteration is smallest. The reconstructed image of 50th iteration using conventional Landweber iterative algorithm was adopted as the initial image for sensitivity matrix update.

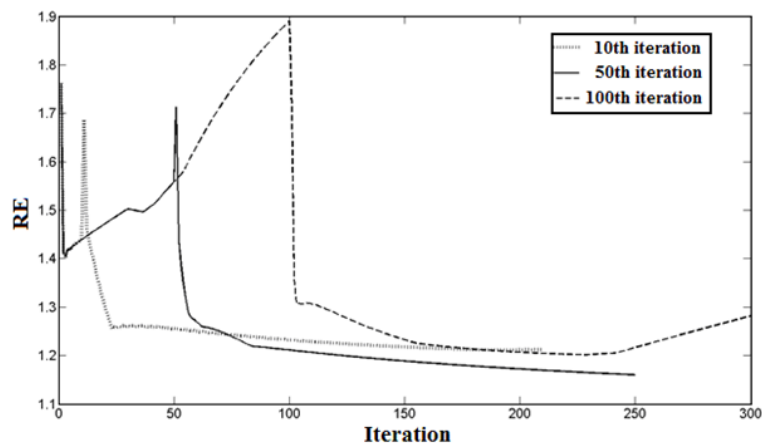


Fig. 5: Numerical result of RE

TIMES OF SENSITIVITY MATRIX UPDATE

Four different phantoms were selected and the reconstructed images of both conventional Landweber iterative algorithm at 50th iteration and Landweber iterative algorithm with 1st, 2nd and 3rd sensitivity matrix update at 50th iteration were shown in figure 6 and the behaviour of RE was also shown in figure 7. It can be seen from figure 7 that the RE was smallest. Usually two times of sensitivity matrix update should be enough.

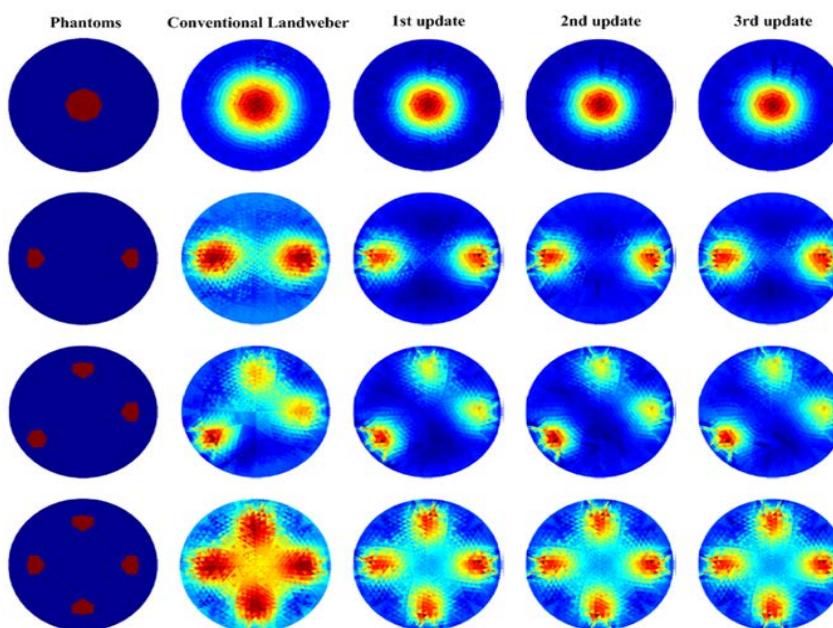


Fig. 6: Different times of sensitivity matrix update

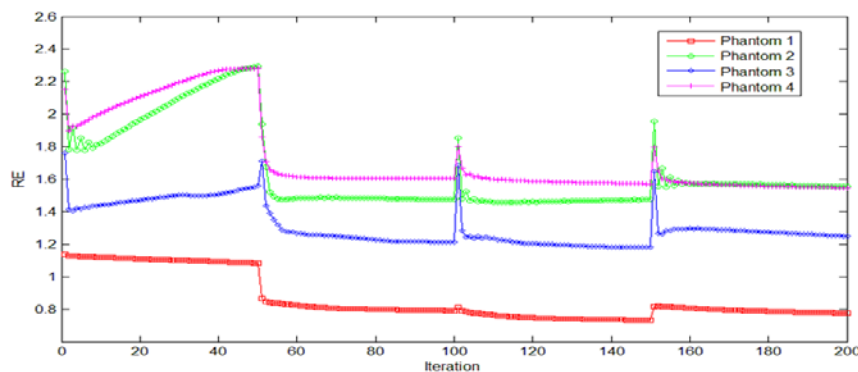


Fig. 7: Numerical result of RE

STATIC TEST

To verify the performance of the presented method, static test was carried out using a FPGA-based ECT system developed by Tianjin University [14]. The excitation signal, demodulation and data acquisition are finished by FPGA.

The static test results were shown in figure 8. For the first test phantom, there were three objects with different size. These three objects cannot be distinguished for the reconstructed image using conventional Landweber iterative algorithm. After 1st update, the quality of reconstructed image was enhanced a little. After 2nd update, these three objects can be distinguished clearly.

For the second test phantom, two objects were close to each other. As the reason of the 'soft-field' effect, these two objects cannot be separated clearly for the reconstructed image. After 2nd update, these two objects can be separated. The quality of reconstructed images was improved after sensitivity matrix update.

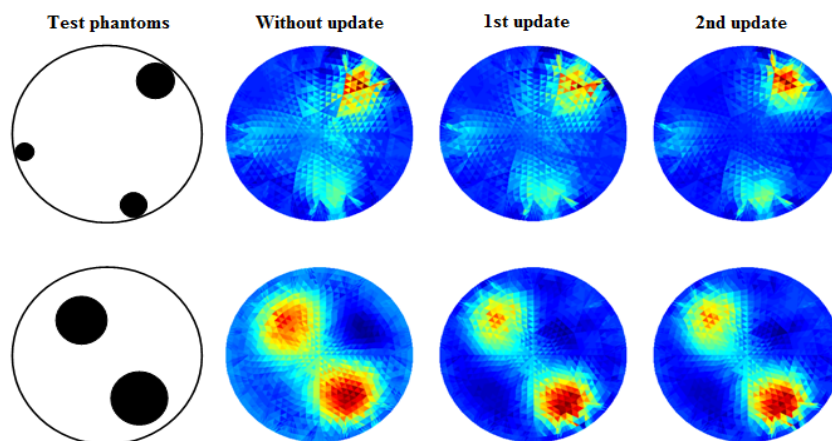


Fig. 8: Static test results

CONCLUSION

This paper presented the sensitivity matrix update strategy for ECT. Simulation and static test results indicated that the quality can be improved. It also can be seen that there is no need to update sensitivity matrix many times and two times update are usually enough. The sensitivity matrix was calculated using the software developed by MATLAB 2007. If the software based on Visual C++ can be used, the calculation time can be further decreased, with which the sensitivity matrix update strategy can be used in more situations.

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